

The in-vitro effects of white henna addition on the *Candida albicans* adhesion and physical properties of denture base resin

Purpose

This *in-vitro* study evaluated and compared the effect of white henna (WH) and natural henna (NH) addition on *Candida albicans* adhesion and physical properties of the denture base material.

Materials and Methods

A total of 243 acrylic resin specimens (9 per group) were divided as follows: 81 for flexural strength, 81 for *Candida albicans* adherence test, and 81 for surface roughness, translucency, and hardness. Heat-polymerized acrylic resin specimens were prepared by adding 0.5, 1.0, 1.5, or 2.0 wt% of WH or NH. *Candida albicans* adhesion was determined using direct culture and slide count methods. Flexural strength, surface roughness, hardness, and translucency were measured using the three-point bending test, profilometer, Vickers hardness test, and spectrophotometer, respectively. ANOVA and post hoc Tukey's tests were performed for data analysis.

Results

Addition of 0.5% WH, 1% WH, and 0.5% NH to denture base resin significantly decreased *Candida albicans* adhesion ($p < 0.05$). WH and NH significantly decreased the flexural strength and translucency, except 0.5% WH, and significantly increased surface roughness, except 0.5% WH and 0.5% NH. WH addition showed non-significant differences in the hardness, while NH addition significantly decreased hardness ($p < 0.05$).







Conclusion

Addition of WH and NH decreased *C. albicans* adhesion to PMMA denture base resin. However, flexural strength, translucency, and surface roughness were adversely affected, particularly at higher concentrations. Hardness was reduced with NH only.

Keywords: Antifungal agent, *Candida albicans*; Dental prosthesis, Henna, Physical properties

Introduction

Polymethylmethacrylate (PMMA) was introduced as a denture base material due to its ease of fabrication, low cost, esthetics, ease of repair, and relatively low toxicity (1). However, the use of the denture intra-orally changes the bio-environment and paves the way for the deposition of biofilms (2). The porous and irregular surfaces of acrylic resins favor microbial adhesion, accumulation, and colonization, which are determining factors in the majority of oral diseases such as candidiasis, sore/burning mouth, and glossodynia (3). Moreover, improper denture hygiene results in debris accumulation and biofilm formation. This leads to inflammatory changes in the underlying mucosa and causes denture-related stomatitis (DS) (4). The role of *Candida albicans* (*C. albicans*) in the development of DS is associated with pathogenic overgrowth of *Candida* on denture sur-

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faces and the oral mucosa, which is widely accepted as an etiological factor (5,6).

The therapeutic strategies currently used to overcome these fungal infections are topical and/or systemic antifungal agents, topical antiseptics, and disinfectants (5). A commonly used antifungal agent known to be an effective treatment of DS is nystatin. However, nystatin is toxic and assists in the development of resistant strains of *C. albicans* (7). Unfortunately, the recurrence of DS may happen due to the short-acting effects of antifungal medications and the low salivary flow rate, making careful cleaning and disinfection of the denture post antifungal treatment crucial (7,8). This led researchers to adopt more incorporative approaches of natural extract-based antifungal agents into the acrylic resin of the denture base (9).

Several natural extract-based antifungal agents products could prevent DS (10-15). These products were found to be less costly, less toxic, and had reduced ability to produce resistant strains compared to pharmaceuticals (10,11). One of these natural antimicrobial products that could be incorporated into denture base is henna (12,13). Many studies have found that henna has an antifungal effect and could be used to treat fungal infections as a substitute to pharmaceuticals (16,17). Henna has been used in many cultures for the health and wellness of skin and hair, and for the treatment of body lesions caused by fungal infections for thousands of years. However, allergic reactions were found to be one of its side effects. Although few cases have been reported, it was declared that henna carries no genotoxic risk, as confirmed by Yusuf *et al.* (18-20).

In a study conducted by Nawasrah *et al.* (14), henna was used as an antifungal agent to prevent the occurrence of DS. This study recommended the use of henna in low concentrations, as high concentrations had an adverse effect on the denture's physical properties, namely color changes (21). Its incorporation in acrylic resin has provided a denture base with antifungal efficacy to control *C. albicans* proliferation (14). However, discoloration of the final product has limited its use. White henna (WH) is a completely synthetic material that originated in the 1970s. According to the manufacturer, WH is a dust powder and is composed of talcum, titanium dioxide, calcium carbonate, and menthol. The product is synthesized to bleach body hair and skin complexion. It is also used as a scrub to remove dead/damaged skin cells. The material also has the ability to withstand temperatures above 200 °C (22). To the best of our knowledge, the effect of WH on denture base resin has not been investigated in the literature. We aimed to investigate the effect of WH on *C. albicans* adhesion as well as the physical properties of PMMA denture base material in comparison to a PMMA/NH composite. First, we propose that WH addition has antifungal effect. Second, we postulate that WH addition has no effect on the physical properties of PMMA and can be used as an alternative to NH for DS prevention.

Materials and Methods

Study design

A prior power analysis revealed that a total of 243 specimens ($n = 9$) were needed to adequately detect the differ-

ences between WH and NH at different concentrations and quantify their effect on the tested properties of modified denture base resin. In accordance with ADA specification No. 12 for denture base polymer, metal molds were prepared in dimensions of 65 × 10 × 2.5 mm for the assessment of flexural strength ($n = 81$) (23). For *C. albicans* adherence test ($n = 81$), surface roughness, hardness, and translucency ($n = 81$), the dimensions of the specimens were 10 × 20 × 2.5 mm. This resulted in a total of 243 specimens of heat-polymerized acrylic resin. The specimens were divided into 9 groups ($n = 9$) according to filler concentration (Table 1). The control group consisted of unmodified acrylic resin, while the other eight tested groups were prepared by addition of either type of henna at different concentrations (0.5%, 1.0%, 1.5 %, or 2.0 wt%) to acrylic powder (Major base 20, Major Prodotti Dentari, SPA, Italy).

White henna addition

WH (white henna, facial bleaching for face and neck, small size - 8850748038009) is a product that has obtained proper registration by the Ministry of Health. Licensed by FDA under registration number por 3/2541 and through por 4/2541. Natural extract of NH (Yamani henna powder, Harazi), was also used in the current study (14,24). An electronic scale was used to weigh the WH or NH, which were added separately to the PMMA powder in plastic beakers and mixed for 1 min. Next, they were mixed with PMMA powder and stirred in a blender at a rotating speed of 400 rpm for 30 min to achieve an equal distribution of henna within the acrylic powder.

Denture base resin preparation

Polymerization was carried out according to the method specified by the manufacturer and as prescribed in a previous study (25). After complete polymerization, the specimens were retrieved and finished by using a tungsten carbide bur (HM 79GX-040 HP; Meisinger) at 18,000 rpm followed by progressively finer cylindrical silicon resin burs (FINOPOL Polishers, 64830, LABOSHOP GmbH, Germany). Similar to the conventional method of denture polishing, only the cameo surfaces were polished by using a polishing cloth disc (TexMet C10in, 42-3210, Buehler GmbH, Germany) on a polishing machine (Metaserve 250 grinder-polisher, Buehler, Germany) at 100 rpm for five minutes under wet conditions (26,27). After ultrasonic cleaning, the specimens were stored for one week at 37 °C in distilled water that was changed daily to reduce residual monomers (28).

For the *C. albicans* adherence assay, specimens were sterilized with 70% alcohol then cleaned ultrasonically with sterilized distilled water. They were then incubated at 37 °C for two days in artificial saliva containing 2,000,000 *C. albicans* cells (ATCC 10231). The specimens were later washed and evaluated for attached and proliferated *C. albicans*. The specimens were incubated in a broth at 37 °C for 48 h after washing each specimen three times with phosphate-buffered saline (PBS). The broth was vibrated using a vortex followed by centrifugation of the tubes containing the specimens to yield a concentrated pellet of *C. albicans*. Later, two methods to count the number of adhered *C. albicans* to acrylic resin sample were used for each specimen.

Direct culture method - colony forming unit (CFU)

A 10 ml amount of each pellet was taken, serially diluted, and spread on a petri dish. The petri dish was incubated at 37 °C for 48 h. Colonies of *C. albicans* were counted using a marker pen counter (colony counter "Scienceware- bel-art products," Wayne, NJ, USA) in the quadrant where acceptable growth was noted and corrected for the dilution factor (14).

Slide count method

The collected candida pellets were placed on a slide count (Nebauer Slide Counter "Chambers-Marienfeld") after adding 2.5 ml of 0.4% solution of trypan blue in phosphate (MP-Biomedicals) to 7.5 ml of each sample for microscopic evaluation. The trypan blue stain can differentiate between dead and living *C. albicans*; dead cells usually appear blue in color while living cells appear transparent with a blue border. Using light microscope at low magnification (10X), the number of *C. albicans* was counted. The slide count usually contained four main squares; each is divided into 16 squares. *C. albicans* was counted in two main squares and multiplied by two to get the total number of *Candida* on the slide.

Physical properties

To determine the flexural strength, fracture load was measured using a three-point bending test on a universal testing machine (Instron, Model 2519-106, Norwood, MA, USA). Each specimen was placed on a 3-point flexure apparatus where the support span was 50 mm. Load was applied at the midpoint of the prepared area with a crosshead speed of 5 mm/min until the specimen fractured, and the maximum load at fracture was recorded. In order to calculate the flexural strength value of each specimen, the following formula was used: $FS = 3WL/2bd^2$ where FS is the flexural strength (MPa), b is the fracture load (N), W is the distance between the two supports, d is the specimen width, and L is the specimen thickness.

The surface roughness value (R_a , mm) was determined using a non-contact optical profilometer (Contour GT, Bruker Nano gmbH, Berlin, Germany). A linear variable differential transformer was installed to measure the surface morphology, while the numerical values of the surface profile were calculated on a computer to obtain the R_a . Three readings per specimen surface were measured (one at a midpoint and two at the margins) on each of the nine specimens per group, and the average R_a was recorded.

The hardness test was conducted using its corresponding tester (Wilson Hardness, ITW Test & Measurement GmbH, Shanghai, China) equipped with a Vickers diamond. An indenter (25-gf load) was applied for 30 s per specimen; the hardness values were digitally recorded for each specimen.

A reflectance value was measured using a spectrophotometer. A small size (10 × 7.5 mm) of aperture viewing area was selected. The spectrophotometer was calibrated using the provided white tile and black trap following the manufacturer's recommendations. Each specimen was stabilized against the port, supported at the back by a white or black reference material with the support arm closed. Color measurements of the coordinates (L^* , a^* , b^*) of the CIE system

were made for every disc against each background. Three readings were made for each specimen and the average was automatically presented by the software. Data was tabulated and translucency was calculated using the following equation $TR = [(L^*white - L^*black)^2 + (a^*white - a^*black)^2 + (b^*white - b^*black)^2]^{1/2}$ (26).

Statistical analysis

Normality in the data set was checked using a Shapiro-Wilk test. The test outcome provided insignificant p -values, proving that the data were normally distributed. Hence, statistical tests used for further analysis were parametric tests. One-way Analysis of variance (ANOVA) was conducted to determine the effects of white henna and natural henna on *C. albicans* adhesion, flexural strength, surface roughness, hardness, and translucency of the modified PMMA denture base resin. Tukey's honestly significant difference (HSD) post hoc test was used to determine differences in measurements between the different denture base materials. The correlation between measurements was tested using Pearson correlation analysis. For all comparisons, statistical significance difference was accepted to be $p < 0.05$.

Results

ANOVA was used to test the overall significance of all properties between all groups (Table 2). After obtaining significant p -values from both WH and NH, pairwise comparisons were done using Tukey's HSD post hoc test (Table 3 and 4). Means, standard deviations, and statistical significances of *Candida* adhesion are summarized in Table 3. The results showed that the amount of *C. albicans* adhesion varied depending on the type of henna and their concentrations according to the variance analysis ($p < 0.05$) (Table 3).

In the direct culture method (Figures 1 and 2), Figure 2 showed that the addition of 0.5% NH and 0.5% WH significantly decreased *C. albicans* adhesion in comparison to the control group ($p < 0.001$) and had a value of (1007.2 ± 44.1) and (561.1 ± 17.0), respectively. However, henna concentrations of more than 0.5%, significantly increased *Candida* adhesion in comparison to the control group ($p < 0.001$). When utilizing the slide count method, it was noted that concentrations of 0.5% and 1.0% of the NH groups and 0.5% of the WH groups significantly decreased the *C. albicans* adhesion compared to the control group ($p < 0.001$), ($p < 0.001$), and ($p < 0.001$) by values of (2268 ± 139.7), (3207 ± 132.5) and (1920.2 ± 69.5), respectively. Other concentration groups (more than 0.5% NH & 1.0% WH) showed a significant increase in *C. albicans* adhesion compared to the control group ($p < 0.01$).

Between the NH and WH groups, a significant difference ($p < 0.001$) was found between all concentration groups except between 1.0% NH and 1.5% WH ($p = 0.18$) groups in terms of direct count. In addition, no significant differences were noted between 0.5% NH and 1.5% NH ($p = 0.994$) as well as 0.5% NH and 1.5% WH ($p = 0.999$), or between 1.5% NH and 1.5% WH ($p = 0.827$) in terms of slide count.

One-way ANOVA revealed NH and WH addition affected flexural strength (Table 2). The results showed that addition of NH and WH showed a statistically significant decrease in

the flexural strength in comparison to the control group ($p < 0.001$), except for the 0.5% WH group as it showed the highest FS value (83.09 ± 0.98 MPa) (Table 4). Comparing NH groups, a significant decrease in FS was found between all groups ($p < 0.001$). FS decreased as NH concentration increased where 2.0% NH had the lowest FS value (57.61 ± 1.20 MPa). Similarly, a significant decrease in FS was found between all groups of WH addition ($p < 0.0001$). FS decreased as WH concentration increased where 2.0% WH had the lowest FS value (59.5 ± 1.02 MPa). When comparing the NH and WH groups the NH and WH groups, significant differences were found between all groups except 0.5% NH and 1.0% WH ($p \approx 1.0$) and between 1.0% NH and 2.0% WH ($p = 0.993$).

One-way ANOVA revealed that NH and WH addition significantly affected surface hardness ($F = 12.978$, $p < 0.001$) (Table 2). The mean surface hardness and standard deviation of tested groups are summarized in Table 4. In comparison to the control group, the results showed a significant decrease in the hardness of all NH groups and 2.0% WH addition ($p < 0.001$) while there was no statistical significant difference at 0.5% WH ($p = 0.601$), 1.0% WH ($p = 0.416$) and 1.5% WH ($p = 0.221$). Additionally, the highest hardness value was reported in the control group (38.67 ± 1.33 VHN). The results showed that the addition of NH to PMMA denture base resin significantly decreased the hardness values in comparison to the control group ($p < 0.001$) while WH addition showed no significant difference in hardness values ($p > 0.05$), except the 2% NH group ($p = 0.022$).

Comparing NH groups, insignificant differences in hardness were found between all groups. The hardness value was lowest in the 1.0% NH group (31.05 ± 2.03 VHN). In between WH groups, insignificant differences in hardness was found between all groups ($p > 0.05$). The lowest hardness value was observed in the 2.0% WH group (35.39 ± 2.28 VHN). In comparison, between the NH and WH groups, insignificant differences were found between the 0.5% NH and 2.00% WH ($p = 0.352$) and the 0.5% NH and all NH groups, where the p -values were: 1.0% NH ($p = 0.334$), 1.5% NH ($p = 1.00$), and 2.0% NH ($p = 0.809$). Also, insignificant differences were found between 1.00% NH and 1.5% NH ($p = 0.413$), 1.5% NH and 2.0% NH ($p = 0.744$), and 1.5% NH and 2.0% WH ($p = 0.289$). There were insignificant differences found between 2.0% NH and all WH groups, where the values were: 0.5% WH ($p = 0.601$), 1.0% WH ($p = 0.416$), 1.5% WH ($p = 0.221$), and 2.0% ($p = 0.998$).

One-way ANOVA results showed that NH and WH additions significantly increased surface roughness ($F = 177.283$, $p = 0.000$) (Table 2). In comparison to the control group, Tukey results (Table 4) showed a significant increase in R_a with NH and WH addition ($p < 0.001$) in all percentages, except for 0.5% NH ($p = 1.00$) and 0.5% WH ($p = 0.999$) addition groups. Addition of 2.0% NH had the highest R_a value (0.51 ± 0.03 μm). When comparing NH groups, a significant increase in R_a in all groups was observed ($p < 0.001$). Similarly, between WH groups, a significant increase in R_a in all groups ($p < 0.001$) was noted. R_a increased as the concentration of NH and WH increased where 2.0% NH had the highest value (0.51 ± 0.03 mm). Non-significant differences were found when NH and WH were compared at 0.5% NH and 0.5% WH ($p = 1.00$), 1.0% NH and 1.0% WH ($p = 0.999$), and at 1.5% NH and 1.5% WH ($p = 0.989$).

One-way ANOVA proved NH and WH addition significantly affected translucency ($F = 370.890$, $p < 0.001$) (Table 2). As shown in Table 4, a significant decrease in the translucency was found with NH and WH additions in comparison to the control group ($p < 0.001$), except for 0.5% WH ($p \approx 1.00$); the control group had the highest translucency value (15.82). Comparing NH groups, a significant decrease in translucency was found between all groups ($p < 0.001$). The translucency value decreased as NH concentration increased and 0.5% NH showed the highest translucency (12.79 ± 0.61) while 2.0% NH showed the lowest translucency value (4.82 ± 0.29). In between the WH groups, in between WH groups, a significant decrease in translucency was noted between all groups, except for 0.5% WH ($p \approx 1.00$). The translucency value decreased as WH concentration increased where 2.0% WH had the lowest translucency value (8.17 ± 0.33). Also, non-significant differences were found between NH and WH for 0.5% NH and 1.0% WH ($p = 0.093$) and 1.0% NH and 1.5% WH ($p = 0.342$).

Discussion

The incorporation of antifungal agents in polymeric materials is considered a good alternative for slow and prolonged

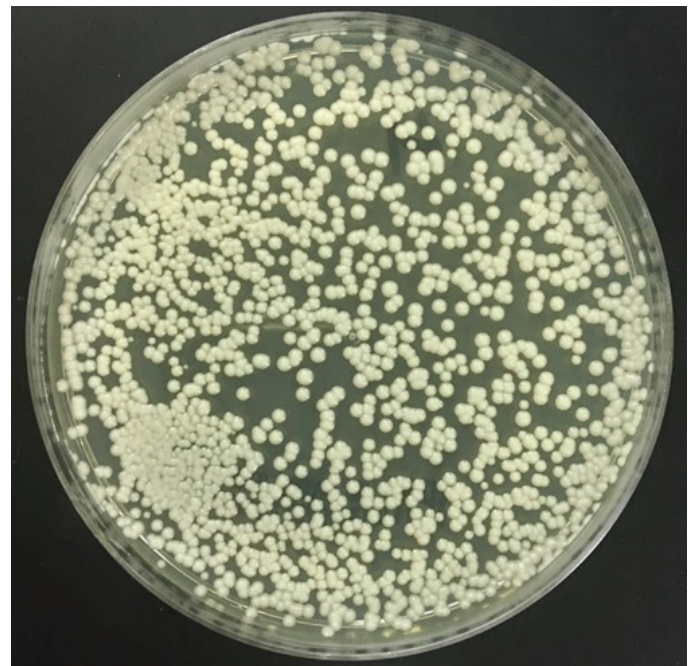


Figure 1. Direct culture method for *Candida* count - control group (unmodified group).

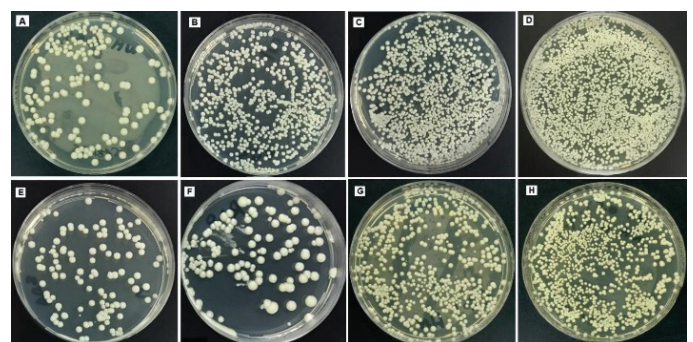


Figure 2. Direct culture method for *Candida* count - Henna modified groups A-D NH group; E-H WH group.

drug release in the mouth and may be therapeutically useful against *C. albicans* since it does not depend on patient cooperation (7,11,12). Moreover, it would maintain constant and prolonged contact of the antifungal agent with the oral tissues. It has been reported that a large portion of topical drugs used in fighting DS are lost from the oral cavity during the first three hours due to the diluting effect of saliva, and the cleaning effect generated by movement of the oral musculature that results in possible reduction of the therapeutic effect (6,8). Consequently, henna addition was suggested to be incorporated into denture base materials (21). This study hypothesized that henna has antifungal effects that may aid in the prevention of DS without compromising the denture base's physical and mechanical properties. This was confirmed through our results, which suggest low concentrations of henna can offer an antifungal activity preventing DS; however, it compromises the physical and mechanical

properties of the denture base to some extent.

Henna is a readily available and cheap powder that has been proven to have some antifungal properties (17). It can be incorporated into the denture's base material in certain concentrations, making it cost effective and able to prevent recurring DS. This method results in what has been called a potential antimicrobial denture base; however, concerns of alterations to the mechanical and physical properties of the denture base rise with such procedure (14,29).

The results of this study have shown that a 0.5% concentration of either WH or NH as well as 1.0% WH reduced *C.*

Table 1. Grouping of the specimens according to NH and WH concentrations.

Group	Specifications
Control	Unmodified acrylic resin
I Natural Henna (NH)	Acrylic resin modified with 0.5% NH
	Acrylic resin modified with 1.0% NH
	Acrylic resin modified with 1.5% NH
	Acrylic resin modified with 2.0% NH
II White henna (WH)	Acrylic resin modified with 0.5% WH
	Acrylic resin modified with 1.0% WH
	Acrylic resin modified with 1.5% WH
	Acrylic resin modified with 2.0% WH

Table 3. Mean (SD) and significant differences of *C. albicans* adhesion count (CFU/mL) according to henna type and concentration. Same lowercase letter in respective column indicated insignificant differences between tested groups whereas the level of significance was 0.05.

Group	%	Mean(SD)	
		Direct culture method	Slide Count method
Control	0	1348.0(23.8)	3265.0(135.3)
	0.5%NH	1007.2(44.1)	2268.0(139.7) ^{a,b}
NH	1.0%NH	2061.4(31.1) ^a	3207.0(132.5)
	1.5%NH	2313.0(167.3)	5462.0(92.2) ^{a,c}
	2.0%NH	3207.0(132.5)	7357(296.4)
WH	0.5%WH	561.1(17.0)	1920.2(69.5)
	1.0%WH	1107.1(12.8)	3311.5(105.1)
	1.5%WH	1565.2(31.6) ^a	4618.5(140.1) ^{b,c}
	2.0%WH	2746.1(114.6)	6706.0(128.9)

Table 2. ANOVA of direct culture, and slide count tests for *Candida* adhesion, flexural strength test, hardness test, surface roughness test, and translucency.

			Sum of Squares	df	Mean Square	F	Sig.
Candida Adhesion	Direct culture	Between Groups	60995760.422	8	7624470.053	1079.225	.000
		Within Groups	572245.900	81	7064.764		
		Total	61568006.322	89			
	Slide count	Between Groups	295844993.622	8	36980624.203	1632.860	.000
		Within Groups	1834468.200	81	22647.756		
		Total	297679461.822	89			
Flexural Strength	Between Groups	6763.106	8	845.388	628.953	.000	
	Within Groups	95.432	71	1.344			
	Total	6858.538	79				
Hardness	Between Groups	411.141	8	51.393	12.978	.000	
	Within Groups	285.116	72	3.960			
	Total	696.257	80				
Surface roughness (Ra)	Between Groups	1.069	8	.134	177.283	.000	
	Within Groups	.054	72	.001			
	Total	1.124	80				
Translucency	Between Groups	1150.665	8	143.833	370.890	.000	
	Within Groups	27.922	72	.388			
	Total	1178.587	80				

Table 4. Mean (SD) and significant differences of flexural strength, hardness, surface roughness, and translucency of tested specimens according to henna type and concentration.

Group	%	Mean(SD)			
		Flexural strength (MPa)	Hardness (VHN)	Surface roughness (μm)	Translucency
Control	0	82.79(1.78) ^a	38.67(1.33) ^a	0.19(0.012) ^a	15.82(1.1) ^a
	0.5%NH	79.67(0.68) ^b	33.23(2.20) ^b	0.19(0.01) ^{a,b}	12.79(0.61) ^b
	1.0%NH	70.80(0.64) ^d	31.05(2.03) ^{b,c}	0.35(0.04) ^c	10.65(0.65) ^c
	1.5%NH	62.57(1.10) ^c	33.12(3.04) ^{b,c,d}	0.41(0.02) ^d	5.91(0.52)
	2.0%NH	57.61(1.20)	34.72(1.02) ^{b,d,e}	0.51(0.03)	4.82(0.29)
NH	0.5%WH	83.09(0.98) ^a	36.52(2.79) ^{a,e,f}	0.20(0.01) ^{a,b}	15.69(0.51) ^a
	1.0%WH	77.77(1.54) ^b	36.78(0.99) ^{a,e,f}	0.35(0.02) ^c	13.65(0.61) ^b
	1.5%WH	71.32(1.10) ^d	37.12(0.81) ^{a,e,f}	0.40(0.02) ^d	11.33(0.69) ^c
	2.0%WH	59.95(1.02) ^c	35.39(2.28) ^{b,d,e,f}	0.46(0.03)	8.17(0.33)

Same lowercase letter in respective column indicated insignificant differences between tested groups whereas the level of significance was 0.05.

albicans adhesion and subsequently, DS, in accordance with previous studies (14,16). While naphthoquinones are considered to be the main active molecules that give natural henna this antifungal property, the antifungal activity of WH is gained from its ingredients: talcum, titanium dioxide, calcium carbonate, and menthol (22). These chemicals were able to withstand the high temperatures PMMA is subjected to during curing (22). Further investigations are still required as WH showed over one-fold greater (55.7%) antifungal activity than NH at the same concentrations (0.5%).

A correlation between surface roughness and *C. albicans* adhesion and colonization has been reported (30). Surface roughness is an important property of the denture base material that influences plaque and microbial adhesion (31,32). A rough denture surface provides more area for microbial adhesion. In addition, it protects entrapped microorganisms from shearing forces during denture cleaning, making their removal difficult even when using antimicrobial agents (33). According to the findings of the current study, as NH and WH concentrations increased, *C. albicans* colonies increased, and this increase in colonies was proportional to the increase in surface roughness reported with modified groups.

The present study has shown that the addition of WH or NH decreases the FS of modified denture base in a direct relation to the filler concentration compared to non-modified denture base. Regardless, the decrease observed in some concentration groups remained above the minimally accepted FS value according to ISO: 1567 standard requirements (65 MPa) (23,34). The groups that met the standard requirement were 0.5%, 1.0%, and 1.5% of WH as well as the 0.5% and 1.0% NH groups. In alignment with previous reports, the addition of low concentrations (0.5%, 1.0%) of thymoquinone antifungal agent did not affect the FS of PMMA denture base material (25).

A significant decrease was also noted in the modified denture base hardness value in all NH groups, which was in agreement with Nawasrah *et al.*, and only the 2.0% concentration of WH groups (24). Unaffected WH groups may be attributed to the synesthetic constituents of WH, where particles were well distributed and bonded to PMMA. This

effect is observed up to 1.5% concentration, above which resin saturation is attained and hardness is decreased.

The decrease in FS and hardness values may be attributed to the additive in the PMMA denture base material since it interferes with the integrity of the polymer matrix (30). These added particles could be aggregate-forming clusters acting as stress-concentration areas within the matrix (22,24). The weak bond between NH and the PMMA resin matrix makes the added henna act as an impurity, which resulted in an adverse effect on the degree of conversion. This, in turn, led to an increase in the level of residual unreacted monomer that acted as a plasticizer (22,35).

The oral tissue conditions under the denture base are affected by the surface properties of the denture base. Previous studies have suggested that surface roughness was found to be directly proportional to microorganism attachment to the denture base (24,32). The results of present study showed that the specimens' R_a values significantly increased as the NH and WH concentrations increased. The increase in R_a values with high henna concentrations might be explained by the presence of some loosely attached particles of NH and WH on the resin surface which could easily be removed during the finishing and polishing phases, leaving voids (22).

The maximum acceptable R_a of removable prostheses for clinical use is 0.2 μm (31). In this study, both NH and WH at 0.5% concentration had lower R_a values (0.19 μm), which is considered clinically acceptable. This suggests that the limit for addition in relation to R_a is 0.5% for both henna types. Nawasrah *et al.*, studied the effect of NH addition to PMMA denture base and noted that surface roughness increased as the percentage of henna increased, in consensus with this study (24).

The success of a removable prosthesis relies on the appearance of the denture base in relation to that of the patient's oral mucosa, and the translucency of the material itself. To offer prosthesis with a natural look, the level of translucency is critical. Therefore, it is important to create a harmonious optical property between the removable prosthesis and the underlying mucosa giving a "chameleon" effect, allow-

ing the underlying soft tissues to show through the PMMA denture base (26). A significant decrease in translucency was noted with NH and translucency decreased as the concentrations of NH increased. On the other hand, 0.5% WH did not change the translucency in comparison to the control group, yet slight changes in translucency were found in 1.0% and 1.5% WH. The difference in the results may be attributed to henna color, where NH was found to be grey and WH was white. This resulted in different color absorption or reflection ability. Specimens with high concentrations of NH seemed black in color, while specimens containing high concentrations of WH appeared white.

White henna showed promising results that might help in the prevention of DS even with the alterations of the physical and mechanical properties of PMMA. This can be achieved when adding WH at 0.5% and 1.0% concentrations. An acceptable concentration of NH was found to be 0.5%, while higher concentrations lead to poor physical and mechanical properties of PMMA. It is recommended that future studies test the antifungal activity of WH at lower concentrations and its effect on the physical and mechanical properties of PMMA. Further investigation including aging effects such as water immersion, thermal cycling, and the longevity of the antifungal effect would also be very interesting and highly beneficial.

Despite some key foundational successes from which to build on, this *in-vitro* study also suffered some limitations. We noted the lack of use of other types of denture base materials; the lack of proper simulation of the oral environment, precluding dynamic movements; thermal changes; saliva with prospective pH; and the presence of other microorganisms that may affect the denture base properties and *C. albicans* adhesion.

Conclusion

Within the limitations of this study, the following conclusions can be drawn: the addition of 0.5%, 1.0% WH, and 0.5% NH to denture base material decreased *C. albicans* adhesion. However, increased concentrations of either type of henna yielded higher *C. albicans* adhesion. The addition of either type of henna decreased the flexural strength, especially at high concentrations. NH addition decreased the hardness, while no change in hardness with WH addition was observed. The addition of 0.5% WH or NH did not affect surface roughness, while higher concentration produced rougher surfaces. NH addition decreased translucency, while 0.5% WH addition did not show any changes in translucency.

Türkçe Özet: Beyaz henna ilavesinin protez kaidesi reçinelerine *Candida albicans* tutunması ve fiziksel özelliklerine *in vitro* etkisi. Amaç: Bu *in-vitro* çalışmada, protez kaide materyaline beyaz henna (BH) ya da doğal henna ilavesinin (DH) *Candida albicans* tutunması incelenmiştir. Ayrıca, bu akrilik materyalinin fiziksel özellikleri de değerlendirilmiştir. Gereç ve Yöntem: Toplam 243 akrilik Reçine örneğin (grup başına 9 örnek), 81'i bükülme dayanımını, 81'i *Candida albicans* tutunumunu, 81'i yüzey pürüzlülüğünü, geçirgenliğini ve sertliğini test etmek için kullanılmıştır. Isı ile polimerime olan akrilikten yapılmış olan örnekler, % ağırlıkça 0.5, 1.0, 1.5, or 2.0 BH ya da NH içerecek şekilde hazırlanmıştır. *Candida albicans* tutunumu, direkt kültür ve koloni sayma yöntemleri uygulanarak ölçülmüştür. Bükülme dayanımı, yüzey pürüzlülüğü, sertliği ve geçirgenliği sırası ile üç-nokta bükme testi, profilometre, Vickers sertlik testi, ve spektrofotometre ile ölçülmüştür. Veri analizi için ANOVA ve post hoc

Tukey's testleri kullanılmıştır ($\alpha = 0.05$). Bulgular: Protez kaide reçinesine 0.5% BH, 1% BH, ya da 0.5% DH ilavesi *Candida albicans* tutunumunu anlamlı şekilde düşürmüştür ($p < 0.05$). BH ve DH, 0.5% lik BH hariç bükülme dayanımı ve geçirgenliği anlamlı şekilde düşürmüştür, 0.5% BH ve 0.5% DH haricinde de yüzey pürüzlülüğünü arttırmıştır ($p < 0.05$). BH ilavesi, sertlikte istatistiksel olarak anlamlı olmayan değişiklikler gösterirken, DH ilavesi sertliği anlamlı olarak azaltmıştır ($p < 0.05$). Sonuç: BH ve DH ilavesi akrilik protez kaide reçinesine *C. albicans* tutunumunu azaltmaktadır. Fakat, bükülme dayanımı, geçirgenlik ve yüzey pürüzlülüğü üzerinde özellikle yüksek konsantrasyonlarda tam ters etki göstermiştir. Sertlik sadece NH ile azalmıştır. Anahtar Kelimeler: Antifungal ajan, *Candida albicans*, Dental protez, Henna, Fiziksel özellikler

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