

https://doi.org/10.51122/neudentj.2024.120

Comparison of Microleakage of Monolithic Zirconia after Surface Treatment and Thermal Cycles Using Data Analysis Software

Emel ARSLAN¹ Halil Nuri ÖZDEMİR2[*](https://orcid.org/0009-0009-9671-5089) Hatice SEVMEZ[3](https://orcid.org/0000-0003-3637-3784)

¹ Ass. Prof., Bolu Abant Izzet Baysal University, Faculty of Dentistry, Department of Prosthodontic, Bolu, Türkiye, emel.arslan08@outlook.com

² Res. Ass., Bolu Abant Izzet Baysal University, Faculty of Dentistry, Department of Prosthodontic, Bolu, Türkiye, ha.halil.nuri1453@gmail.com

³ Ass. Prof., Bolu Abant Izzet Baysal University, Faculty of Dentistry, Department of Prosthodontic, Bolu, Türkiye, hsevmez@hotmail.com

Monolitik Zirkonyaların Yüzey İşlemleri ve Termal Siklus Sonrasında Mikrosızıntılarının Veri Analizi Yazılımıyla Karşılaştırılması

https://doi.org/10.51122/neudentj.2024.120

***Corresponding Author:** Halil Nuri ÖZDEMİR, *ha.halil.nuri1453@gmail.com*

This article is licensed under a Creative Commons Attribution-NonCommercial 4.0 International License (CC BY-NC 4.0)

INTRODUCTION

Resin composites are commonly utilized in clinical dental practice due to their superior mechanical properties, excellent adhesion to tooth structures, ease of application, aesthetic appeal, and compatibility with minimally invasive dental techniques.1,2 These materials offer the distinct advantage of reparability over time, as opposed to complete replacement of damaged restorations. Repair procedures mitigate the drawbacks of full replacement, which often involve extensive preparation and high costs.³

Clinically, crowns have been observed to experience issues such as crumbling and delamination after prolonged use, which leads to restoration failures.⁴ Advances in materials science have introduced high-purity, highly translucent yttria-stabilized tetragonal zirconia polycrystalline (Y-TZP) ceramics, which address the typical limitations of zirconia ceramics, such as inadequate translucency and a monolayer appearance.⁵ To establish a strong bond between tooth structures and porcelain restorations, various surface treatments are employed. Acid etching is one such method, although it is less effective with zirconia restorations due to their structural properties.⁶⁻⁸ Various methods, such as etching, laser irradiation, and nano-grade aluminum coating, are used to create surface roughness that enhances the micromechanical bond between the zirconia and the resin cement.⁹

Despite these modifications, the micromechanical bond remains insufficient, thus necessitating the use of primers with resin cements. For optimal cementation of zirconia restorations, self-adhesive, resin-based agents and universal adhesives containing 10 methacryloyloxydecyl dihydrogen phosphate (10-MDP) are recommended.¹⁰ Other surface treatments, such as tribochemical silica coating—which involves air-etching the ceramic surface with alumina particles coated with silica-have been developed to enhance the bonding between resin cement and zirconia.¹¹ Abrasion with diamond milling is a method frequently used on the fracture surface when repairing in the mouth. Abrasion removes contamination from the fracture surface. It also provides a mechanical connection by providing visibly rougher surfaces than other methods.¹²

Microleakage testing of dental materials is a generally accepted technique for the evaluation of margin integrity. Microleakage refers to the clinically undetectable passage of bacteria, fluids, molecules, or ions in the microgaps $(10^{-6} \mu m)$ between a cavity wall and the restorative material applied over it. The evaluation of microleakage is conducted using the basic fuchsin stain methylene blue.¹³

While there is a relative of studies examining the durability of monolithic zirconia following repair, there is a significant gap in the literature about microleakage and surface treatments. This study aimed to evaluate the impact of different surface treatments on the repair of aged resin composites using monolithic zirconia. The null hypothesis was that there would be no significant difference between the microleakage of disc-shaped specimens repaired with various aged monolithic zirconia materials and surface treatments.

MATERIAL and METHODS

Preparation of the Samples

Three types of monolithic zirconia blocks with different translucency properties were used: multilayered (ML), ultra super translucent multilayered (UTML), and super translucent multilayered (STML) (Table 1). Power and sample size analysis for 'f test - ANOVA: Fixed effects, special, main effects, and interactions' was conducted using G*Power v3.1.9.2. Sample size was determined by referencing the study according to the 95% confidence interval (CI; 1- α), 95% test power (1- β), effect size f=0.374 and analysis of variance (ANOVA)

test.¹⁴ A total of 120 samples were included in the study. All were of the same brand (Katana; Kuraray, Noritake Dental Inc, Tokyo, Japan) and were manufactured using a CAM (Yenadent D43, Yenadent Ltd, İstanbul, Türkiye) system. The sample was designed using computer software (Meshmixer, California, USA) and pre-sintered in a laboratory with a sintering furnace (Everest Therm; KaVo Dental GmbH, Biberach, Germany) following the manufacturer's instructions. According to the international standard ISO 6872, the final dimensions were in the form of a disk 15 mm in diameter and 1.2 mm in thickness, consistent with the methodology used in scientific studies on the durability of all-ceramic materials (Figure 1).¹⁵

The thickness of the samples was checked using a digital caliper. The prepared ceramic samples were ultrasonically washed for two minutes, then air-dried and prepared for surface treatment.

Figure 1. Preparation of Specimens

Material	Code	Manufacturer	Composition	Flexural Strength (MPa)	
Multilayer	ML.	Kuraray, Noritake ZrO_2 + HfO ₂ + Y ₂ O ₃) > 99%, (Y_2O_3) 4%, $(HfO_2) \leq 5\%$, other Dental Inc., Tokyo, oxides $\leq 1\%$ Japan		1125	
Supertranslucent	STML	Kuraray, Noritake Dental Inc., Tokyo, Japan	$(ZrO2 + HfO2 + Y2O3) >99 %$ (Y_2O_3) 5.3 %, (HfO ₂) \leq 5 %, other oxides $\leq 1\%$	748	
Ultratranslucent	Kuraray, Noritake Dental Inc., Tokyo, UTML Japan		$(ZrO2 + HfO2 + Y2O3) >99 %$ (Y_2O_3) 5.4 %, (HfO ₂) \leq 5 %, other oxides $\leq 1\%$	557	

Table 1. Materials used in the study, manufacturer, composition and flexural strength.

Surface Treatment of the Samples

The prepared samples were randomly divided into five groups. For group C (the control group), no surface treatment was applied to the samples. For group HF (hydrofluoric acid), 9% HF (Ultradent Porcelain Etch; Ultradent Inc., South Jordan, USA) was applied to the samples and left for 60 seconds. After two minutes of washing, the HF was removed. Silane (Ultradent, Utah, USA) was then applied to the sample surfaces and allowed to dry for 60 seconds. For group T, tribochemical silica coating was applied. Samples were roughened with 30 um silicacoated Al₂O₃ particles (3M ESPE, Seefeld, Germany) for 15 seconds under 3 bars of pressure.¹⁶ A distance of 10 mm was left between the application tip of the blasting

the silica-coated samples were cleaned with 96% isopropyl alcohol using an ultrasonic device (Euronda, Sassuolo, Italy). For group HF+T, HF and tribochemical silica coating were applied. A 9% HF solution was applied to the samples and allowed to remain for 60 seconds. After two minutes of washing, the HF was removed. Silane was then applied to the sample surfaces and allowed to dry for 60 seconds. The surfaces were then roughened with 30 μ m silica-coated Al₂O₃ particles for 15 seconds under 3 bars of pressure. A distance of 10 mm was left between the application tip of the silica coating and the sample. After the procedure, the silica-coated samples were cleaned with 96% isopropyl alcohol using an ultrasonic device.

device and the sample. All operations were performed by a single user. After the procedure,

Group F+HF+T involved the use of milling burs and HF as well as tribochemical silica coating applications. The samples were roughened by abrading in the same direction for ten seconds with finger pressure by the same operator using 125 μm green-banded diamond burs (Acurata, Thurmansbang, Germany) with a high-speed water-cooled clinical aerator (NSK, Nagaoka, Japan). The device was calibrated by a dental technician with professional assistance. Self-adhesive resin cement (Panavia SA Cement, Kuraray, Osaka, Japan) was bonded to the surfaces with special molds prepared for standardization. A mold with a diameter of 15 mm and a thickness of 2.5 mm was created using pink wax (Polywax, München, Germany). This mold was placed in silicone impression material (Zhermack, Badia Polesine, Italy). The samples, after the adhesive was applied, were then placed in the mold. The polymerization process was performed with an LED (light emitting-diode) light device (Bredent GmbH & Co KG, Senden, Germany) for 40 seconds. The measurements of luminous flux, luminous intensity, and energy density from the LED device were recorded with the Bluephase meter II radiometer (Ivoclar Vivadent, Schaan, Switzerland), and the accuracy was determined by comparison with the technical specifications and standards of the LED device itself. Next, the repair material was removed from the mold. After being bonded to each other with adhesive systems, the samples were soaked in 37°C distilled water for 24 hours and thermal-cycled to mimic aging. The samples were subjected to the aging procedure through a 10.000-cycle thermodynamic cycler (Gökçeler Makine, Sivas, Türkiye) at 5–55°C with a 30-second dwell time.¹⁷

Evaluation with a Microscope

Two coats of blue nail polish (Flormar, Kocaeli, Türkiye) were applied to all areas of the zirconia, except for 1 mm of the connection area. To evaluate marginal leakage, the samples

were soaked in 0.5% basic fuchsin at 37°C for 24 hours. After staining, the prepared samples were cut in half to evaluate the microleakage. Using a linear precision saw (Isomet 1000 Linear Precision Saw; Beuhler, Illinois, USA), the specimens were cut in half at a speed of 600 rpm. The cutting process took into account the thickness of the water-cooled cutting blade, which is 0.3 mm. The prepared samples were kept in basic fuchsin solution for one day to evaluate the coloration of the microleakage areas. Then, images of the samples were taken under a stereomicroscope (SZx10 Olympus, Tokyo, Japan) at 25x magnification) (Figure 2). Calibration was performed by placing a ruler within the field of view of the microscope and utilizing the microscope's measurement capabilities. Surface images were captured once the ruler's measurements were aligned with the measurements provided by the microscope's software. The images were transferred to a computer program (Pycharm 3.12.3, Prague, Czech Republic), and the dimensional sizes of the images were obtained in square millimeters (mm²) through the program (Figure 3).

Statistical Analysis

Statistical analyses were performed using the SPSS software (IMB SPSS Statistics for Windows version 14.0; IBM Corp., New York, USA). To assess the homogeneity of the composite and thickness variance distributions for each group $(n = 8)$, the Shapiro-Wilk test was applied, and normal distributions were found. The measurement values for the monolithic zirconia types and the surface treatments were analyzed using a two-way ANOVA test, and the obtained values were compared using Tukey's test. The p-value's significance level was determined to be $p<0.05$.

Figure 2: Images of samples under the microscope

Figure 3. Measurement of microleakage areas in the Pycharm program

RESULTS

A two-way ANOVA test showed a significant difference in the microleakage values of the monolithic zirconia types and the surface treatments (p<0.001) (Table 2). Table 3 presents the mean microleakage values and standard deviations (SD) of the monolithic zirconia types and the surface treatments. Group F+HF+T exhibited lower microleakage values compared to other surface treatments $(p<0.05)$. When compared with other surface treatments, significant differences were observed among all groups ($p < 0.05$). The lowest microleakage was observed in the control group. A significant difference was found between zirconia grades

for control and HF-treated surfaces ($p < 0.001$). However, no significant difference was observed between UTML and STML on tribochemical silica-coated surfaces (p≥0.05). The lowest microleakage value was obtained for UTML zirconia in the F+HF+T group (12.15 ± 1.69) , while the highest microleakage value was found for ML zirconia in the control group (73.93±1.59). No significant difference was observed between zirconia types in the control group ($p \ge 0.05$), but significant differences were found between zirconia types when surface treatments were applied $(p<0.05)$. Additional multiple comparison results are presented in Table 3 and Figure 4.

	Type III Sum of					Partial Eta
Microleakage	Squares	df	Mean Square	F	Sig.	Squared
Corrected Model	66892.136 ^a	14	4778.010	1106.864	< 0.001	0.993
Intercept	202517.827		202517.827	46914.874	< 0.001	0.998
Material	1347.706	$\mathcal{D}_{\mathcal{L}}$	673.853	156.103	< 0.001	0.748
Surface Treatment	64967.154	4	16241.789	3762.540	< 0.001	0.993
Material * Surface	577.276	8	72.160	16.716	< 0.001	0.560
Treatment						
Error	453.254	105	4.317			
Total	269863.218	120				
Corrected Total	67345.391	119				

Table 2: Two-way ANOVA Test for the Effect of Monolithic Zirconia Types and Surface Treatments on Microleakage

a. R Squared = .993 (Adjusted R Squared = .992)

Table 3: Microleakage Descriptive Statistics

A-E: No difference between surface treatment with the same letter. a-ı: No difference between zirconia types and surface treatment interactions with the same letter.

Figure 4. Boxplot of Microleakage values according to zirconium

DISCUSSION

The results of this study revealed that the surface treatment techniques significantly affected the microleakage values after the repair procedures were performed on the monolithic zirconia ($p<0.05$). The highest mean marginal compliance values were observed in the burs+HF+ tribochemical silica coating treatments. Therefore, the null hypothesis tested in this study was rejected because our findings showed that there was a significant difference between the microleakage values of the

monolithic zirconia that was repaired using different surface treatments. In this study, a diamond bur of silica-coated aluminum oxide was used for mechanical surface roughening. The use of bonding agents increases the bond strength of the repair bonds.

Most clinicians prefer to use the bonding system that they already have in their practice rather than acquire a specialized bonding system for composite repair procedures.¹⁸⁻²⁰ However, the bonding potential of zirconia restorations is low, and there is no standard repair procedure. Different resin cements have been proposed for the repair of these restorations.21,22

The silica coating has been observed to produce microcracks on the surface of zirconia ceramics, increasing their strength.²³ The porcelain and the silane form a chemical connection when the silica creates a glassy coating on the ceramic surface. The results of our study corroborated this finding, as tribochemical silica coating demonstrated a higher level of agreement compared to the other groups. In study, the marginal compatibility with the tribochemical silica coating was significantly increased compared to the control and HF treatments. This is due to the fact that the tribochemical silica coating provides chemical retention with the silica-coated zirconia surface because it binds to the silane more effectively than silica coating.^{24,25} According to a recent study, the use of HF etching on both glass matrix and crystal surfaces resulted in the highest bond strength.²⁶ Moreover, the application of silane and HF to the ceramic surface prior to cementation has been documented to significantly enhance the bonding efficacy of silica-based ceramics. $27,28$ However, it has been shown that the lack of a glassy phase or high crystal content causes HF etching to fail in ceramics reinforced with zirconia and alumina.²⁹ Ural et all.³⁰ found that HF application did not cause any changes in zirconia surface morphology. According to the results of the present study, the HF-treated groups exhibited reduced microleakage in surface marginal areas compared to the control group.

In HF applications, the protocols can vary considerably, particularly in terms of etching time and acid concentration.^{31,32} These variations complicate the assessment of the definitive advantages of this surface treatment, making it challenging to establish a standardized approach for optimal bonding outcomes. In a systematic review, it was concluded that surface treatments with tribochemical silica particles and HF acid resulted in lower coupling than etching with Al_2O_3 or diamond bur abrasives.³³ The current study contradict is incompatible with that systematic review. However, in this study, tribochemical silica coating and diamond milling were used together to reduce microleakage. In clinics, the combination of the two surface treatments may be preferred as a surface treatment for monolithic zirconia repairs.

Prolonged exposure of Y-TZP zirconia to low temperatures may cause different disadvantages. One of these is surface roughness. In addition, reduced durability results in bending force resistance that is sufficient to withstand chewing forces.³⁴ The addition of a stabilizer containing Y_2O_3 as a component to the zirconia material can significantly improve the mechanical properties of zirconia and enhance its biological properties.³⁵ In the results of the current study, UTML (5.4% Y_2O_3), with the highest Y_2O_3 content, showed the least microleakage (12.15 ± 1.69) , while ML $(4\%$ Y₂O₃), with the lowest stabilizer content, showed the highest microleakage values among all of the surface treatments. The results suggest that increasing the Y_2O_3 ratio may enhance the marginal compatibility of the material.

In addition, different sintering temperatures are likely to change the edge fit due to shrinkage as ceramic materials cool to room temperature.³⁶ This shrinkage depends on several factors, including material composition, density, and the sintering procedure.³⁷ Ersoy et all.³⁸ found that increasing the sintering temperature and decreasing the sintering time improve the mechanical properties of the zirconia structure. The sintering temperature of ML monolithic zirconia used in the current study was 1500°C, while the sintering temperature of the STML and UTML monolithic zirconia was 1550°C, as specified by the manufacturer. The differences in the microleakage values of the different experimental groups in this study may have been due to the stability of the zirconia samples and structural differences. With an increase in the sintering temperature, the zirconia samples were found to be completely sintered until the tetragonal stage, and no transformation was observed until the monoclinic stage.38,39 New generation zirconia types include 4Y-PSZ (Katana ML), 5Y-PSZ (Katana STML), and 6Y-PSZ (Katana UTML). In modern dentistry,

the content of Y_2O_3 , the proportion of tetragonal or cubic phases, and the material's fracture toughness are crucial factors for clinical applications. The addition of Y_2O_3 to ZrO_2 powder significantly increases the cubic $ZrO₂$ phase. While this improves certain properties, it can reduce both flexural strength and fracture toughness.⁴⁰

In this study, thermal cycling was applied for 10,000 cycles, which is equivalent to one year. However, D'Amario et all.⁴¹ reported that thermal cycling significantly reduced the bond strength between zirconia and resin cement. In another study, thermal cycling with 10,000 cycles had no effect on bond strength, and even veneer ceramics showed higher bond strength after thermal cycling. In the present study, applying too many thermal cycles was found because it reduced bond strength.⁴²

Additionally, the dye penetration method is often preferred in microscope studies due to its cost and ease of application.⁴³ In the current study, microleakage values were compared using the PyCharm 3.12.3 software to ensure objectivity, rather than relying on traditional scoring methods. Although AutoCAD software was used in previous studies, the data obtained with this program were automatically calculated numerically.14,44,45

The chief limitation of this study is that the oral environment cannot be replicated using different surface treatments and monolithic zirconia with different components. However, this study can guide future in-vivo and in-vitro studies. It will also inform clinicians about the microleakage that may occur after the preferred surface treatment for monolithic restoration repair.

CONCLUSIONS

Conclusions obtained as a result of the limitations of the study; Mechanical and chemical treatments applied to the surface during the repair of monolithic restorations help reduce the risk of microleakage. The components of the monolithic material influence the microleakage values. For minimizing the risk of microleakage, it is recommended that clinicians use monolithic zirconia with high Y_2O_3 content with processes such as tribochemical silica coating and milling.

Ethical Approval

This in-vitro study does not require ethics committee approval.

Financial Support

The authors declare that this study received no financial support.

Conflict of Interest

The authors deny any conflicts of interest related to this study.

Author Contributions

Design: EA, HS, Data collection or data entry: EA, HS, Analysis and interpretation: EA, HS, Literature review: EA, Writing: EA, HNÖ, HS.

REFERENCES

- 1. Joulaei M, Bahari M, Ahmadi A, Oskoee SS. Effect of different surface treatments on repair micro-shear bond strength of silica-and zirconia-filled composite resins. J Dent Res Dent Clin Dent Prospects. 2012;6:131-7.
- 2. Mamanee T, Takahashi M, Nakajima M, Foxton RM, Tagami J. Initial and longterm bond strengths of one-step self-etch adhesives with silane coupling agent to enamel-dentin-composite in combined situation. Dent Mater J. 2015;34:663-70.
- 3. Nassar M, Al-Fakhri O, Shabbir N, Islam MS, Gordan VV, Lynch CD, et all. Teaching of the repair of defective composite restorations in Middle Eastern and North African Dental Schools. J Dent. 2021;112:103753.
- 4. Rekow E, Silva N, Coelho P, Zhang Y, Guess P, Thompson V. Performance of dental ceramics: challenges for improvements. J Dent Res. 2011;90:937- 52.
- 5. Tang Z, Zhao X, Wang H, Liu B. Clinical evaluation of monolithic zirconia crowns

for posterior teeth restorations. Medicine. 2019;98:e17385.

- 6. Pereira GKR, Graunke P, Maroli A, Zucuni CP, Prochnow C, Valandro LF, et all. Lithium disilicate glass-ceramic vs translucent zirconia polycrystals bonded to distinct substrates: Fatigue failure load, number of cycles for failure, survival rates, and stress distribution. J Mech Behav Biomed Mater. 2019;91:122-30.
- 7. Soares PM, Cadore-Rodrigues AC, Borges ALS, Valandro LF, Pereira GKR, Rippe MP. Load-bearing capacity under fatigue and FEA analysis of simplified ceramic restorations supported by Peek or zirconia polycrystals as foundation substrate for implant purposes. J Mech Behav Biomed Mater. 2021;123:104760.
- 8. Stawarczyk B, Keul C, Eichberger M, Figge D, Edelhoff D, Lümkemann N. Three generations of zirconia: From veneered to monolithic. Part I. Quintessence Int. 2017;48:369-80.
- 9. Buyukerkmen EB, Bozkurt DA, Terlemez A. Effect of surface treatment, ferrule height, and luting agent type on pull-out bond strength of monolithic zirconia endocrowns. J Oral Sci. 2022;64:279-82.
- 10. Shin YJ, Shin Y, Yi YA, Kim J, Lee IB, Cho BH, et all. Evaluation of the shear bond strength of resin cement to Y‐TZP ceramic after different surface treatments. Scanning: Scanning Microsc. 2014;36:479-86.
- 11. Heikkinen TT, Matinlinna JP, Vallittu PK, Lassila LV. Dental zirconia adhesion with silicon compounds using some experimental and conventional surface conditioning methods. Silicon. 2009;1:199-202.
- 12. Han I-H, Kang D-W, Chung C-H, Choe H-C, Son M-K. Effect of various intraoral repair systems on the shear bond strength of composite resin to zirconia. J Adv Prosthodont. 2013;5:248-55.
- 13. Kidd EA. Microleakage: a review. J Dent. 1976;4:199-206.
- 14. Günay A, Eskibağlar M, Cangül S, Karaağaç Eskibağlar B, Adıgüzel Ö,

Çelenk S. İki Farklı Işık Cihazı ile Polimerize Edilen Bonding Ajanların Mikrosızıntılarının AutoCAD Programı Kullanılarak Değerlendirilmesi. 7tepe Dent J. 2023;19:173-8.

- 15. ISO I. 6872: Dentistry-ceramic materials. Switzerland: International Organization for Standardization. 2008.
- 16. Çağlar İ, Ateş SM, Arslan E, Duymuş ZY. Farkli Yöntemlerle Üretilen Metal Alt Yapilara Kompozit Rezin Bağlantisi. J Dent Fac Ataturk Univ. 2021;31:414-9.
- 17. Gale M, Darvell B. Thermal cycling procedures for laboratory testing of dental restorations. J Dent. 1999;27:89- 99.
- 18. Burrer P, Costermani A, Par M, Attin T, Tauböck TT. Effect of varying working distances between sandblasting device and composite substrate surface on the repair bond strength. Materials. 2021;14:1621.
- 19. Yin H, Kwon S, Chung SH, Kim RJY. Performance of universal adhesives in composite resin repair. BioMed Res Int. 2022;2022:7663490.
- 20. Wendler M, Belli R, Panzer R, Skibbe D, Petschelt A, Lohbauer U. Repair bond strength of aged resin composite after different surface and bonding treatments. Materials. 2016;9:547.
- 21. Valandro LF, Özcan M, Amaral R, Vanderlei A, Bottino MA. Effect of testing methods on the bond strength of resin to zirconia-alumina ceramic: microtensile versus shear test. Dent Mater J. 2008;27:849-55.
- 22. Akay C, Çakırbay Tanış M, Şen M. Effects of hot chemical etching and 10‐ metacryloxydecyl dihydrogen phosphate (MDP) monomer on the bond strength of zirconia ceramics to resin‐based cements. J Prosthodont. 2017;26:419-23.
- 23. Zhang Y, Lawn BR, Malament KA, Thompson VP, Rekow ED. Damage accumulation and fatigue life of particleabraded ceramics. Int J Prosthodont. 2006;19:442-8.
- 24. Amaral R, Özcan M, Bottino MA, Valandro LF. Microtensile bond strength

of a resin cement to glass infiltrated zirconia-reinforced ceramic: the effect of surface conditioning. Dent Mater. 2006;22:283-90.

- 25. Altan B, Cinar S, Tuncelli B. Evaluation of shear bond strength of zirconia-based monolithic CAD-CAM materials to resin cement after different surface treatments. Niger J Clin Pract. 2019;22:1475-82.
- 26. Bona AD, Anusavice KJ. Microstructure, composition, and etching topography of dental ceramics. Int J Prosthodont. 2002;15:159-67.
- 27. Thompson JY, Stoner BR, Piascik JR, Smith R. Adhesion/cementation to zirconia and other non-silicate ceramics: where are we now? Dent Mater. 2011;27:71-82.
- 28. Seto KB, McLaren EA, Caputo AA, White SN. Fatigue behavior of the resinous cement to zirconia bond. J Prosthodont. 2013;22:523-8.
- 29. Aboushelib MN, Kleverlaan CJ, Feilzer AJ. Selective infiltration-etching technique for a strong and durable bond of resin cements to zirconia-based materials. J Prosthetic Dent. 2007;98:379-88.
- 30. Ural Ç, Külünk T, Külünk Ş, Kurt M. The effect of laser treatment on bonding between zirconia ceramic surface and resin cement. Acta Odontol Scand. 2010;68:354-9.
- 31. Gul P, Altınok-Uygun L. Repair bond strength of resin composite to three aged CAD/CAM blocks using different repair systems. Acta Odontol Scand. 2020;12:131.
- 32. Bayraktar Y, Arslan M, Demirtag Z. Repair bond strength and surface topography of resin‐ceramic and ceramic restorative blocks treated by laser and conventional surface treatments. Microsc Res Tech. 2021;84:1145-54.
- 33. da Rosa LS, Pilecco RO, Soares PM, Rippe MP, Pereira GKR, Valandro LF, et all. Repair protocols for indirect monolithic restorations: a literature review. PeerJ. 2024;12:e16942.
- 34. Pereira GK, Guilardi LF, Dapieve KS, Kleverlaan CJ, Rippe MP, Valandro LF. Mechanical reliability, fatigue strength and survival analysis of new polycrystalline translucent zirconia ceramics for monolithic restorations. J Mech Behav Biomed Mater. 2018;85:57- 65.
- 35. Hao Z, Ma Y, Liu W, Meng Y, Nakamura K, et all. Influence of low-temperature degradation on the wear characteristics of zirconia against polymer-infiltrated ceramic-network material. J Prosthet Dent. 2018;120:596-602.
- 36. Hjerppe J, Vallittu PK, Fröberg K, Lassila LV. Effect of sintering time on biaxial strength of zirconium dioxide. Dent Mater. 2009;25:166-71.
- 37. Khaledi AAR, Vojdani M, Farzin M, Pirouzi S. The effect of sintering program on the compressive strength of zirconia copings. J Dent. 2018;19:206-11.
- 38. Ersoy NM, Aydogdu HM, Degirmenci BÜ , Çökük N, Sevimay M. The effects of sintering temperature and duration on the flexural strength and grain size of zirconia. Acta Biomater Odontol Scand. 2015;1:43-50.
- 39. Mohaghegh M, Baseri S, Kalantari MH, Giti R, Ghoraishian SA. Influence of Sintering Temperature on the Marginal Fit and Compressive Strength of Monolithic Zirconia Crowns. J Dent. 2022;23:307-13.
- 40. Kontonasaki E, Giasimakopoulos P, Rigos AE. Strength and aging resistance of monolithic zirconia: an update to current knowledge. Jpn Dent Sci Rev. 2020;56:1-23.
- 41. D'Amario M, Campidoglio M, Morresi AL, Luciani L, Marchetti E, Baldi M. Effect of thermocycling on the bond strength between dual-cured resin cements and zirconium-oxide ceramics. J Oral Sci. 2010;52:425-30.
- 42. Blatz MB, Bergler M, Ozer F, Holst S, Phark J-H, Chiche GJ. Bond strength of different veneering ceramics to zirconia and their susceptibility to thermocycling. Am J Dent. 2010;23:213-6.
- 43. Bahari M, Mohammadi N, Alizadeh Oskoee P, Savadi Oskoee S, Davoodi F. Effect of an extra layer of hydrophobic resin on the microleakage of Cl V composite resin restorations with a universal adhesive system. J Investig Clin Dent. 2017;8:e12234.
- 44. Wahab F, Abu-Tabra IT, Amin WM. An in vitro study of micro leakage of different types of composites with respect to their matrix compositions. JAMMR. 2014;4:1908-22.
- 45. Bolgül B, Ayna B, Şimşek İ, Celenk S, Şeker O, Kılınç G. Leakage testing for different adhesive systems and composites to permanent teeth. Niger J Clin Pract. 2017;20:787-91.