

Evaluation of Shore A hardness of maxillofacial silicones: the effect of dark storage and nanoparticles

Purpose

Little has been reported how the addition of nanoparticles could affect the hardness of maxillofacial silicones. The purpose of this study was to evaluate the effects of different types of nanoparticle additives and dark storage for 2-years on the Shore A hardness of two types of maxillofacial silicone elastomers.

Materials and Methods

A-2000 and A-2006 Room Temperature Vulcanized (RTV) silicone elastomers were tested in this study. Silaned silica, fumed silica and titanium dioxide nanoparticles at concentrations of 10% by volume were used as fillers for the maxillofacial silicone elastomers. A total of 64 silicone specimens were fabricated, which includes 8 samples, 30 x 10 mm in size, from each silicone elastomers for each subgroup and also controls. After the initial Shore A hardness measurements, specimens were kept in dark conditions at room temperature for 2 years. The final measurements were then taken from the silicone specimens. All data were statistically analyzed.

Results

For both types of silicones, there was statistically significant differences among study groups ($p < 0.001$). Fumed silica group showed the lowest hardness values in A-2000 after storage. However, no significant difference was observed between control and fumed silica groups. Control group showed the lowest hardness values in A-2006, while the highest hardness values were found in fumed silica group; there was no significant difference between silica and silane groups.

Conclusion

Shore A values of the specimens were within the acceptable range for the maxillofacial silicones after aging. Nanoparticle addition did not prevent hardening of the silicone elastomers with time.

Keywords: Aging; hardness; nanoparticles; silicone elastomers; Shore A

Pınar Çevik 

Introduction

Maxillofacial prostheses are still being used to treat congenital and acquired defects of the head and neck region, despite advances in plastic surgery (1, 2). Maxillofacial prostheses provide a practical alternative by giving patients a normal appearance, esthetics, and social acceptance (3, 4). Currently, several types of materials can be used in maxillofacial prosthodontics such as chlorinated polyethylene, polymethylmethacrylates, polyurethanes, latex, and silicone elastomers. Silicone elastomers are widely used because of their favorable properties, including acceptable tear and tensile strengths, chemical inertness, high elongation percentage, ease of manipulation and biocompatibility (5, 6). Despite their wide use, they also suffer from deterioration of color and loss of physical, mechanical as well as dynamic properties in clinical practice. The average service life of a maxillofacial prosthesis ranges therefore from 6 to 18 months (6).

ORCID ID of the author: PÇ. 0000-0003-1970-7543

Department of Prosthodontics, Gazi University Faculty of Dentistry, Ankara, Turkey

Corresponding Author: Pınar Çevik
E-mail: dt_pinarcevik@yahoo.com

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Limited research has been conducted to enhance the mechanical and physical properties of maxillofacial silicones by adding nanoparticles (1, 7). Nanoparticles could diffuse the silicone matrix, which leads to the formation of the three-dimensional network within the silicone chain (3, 7).

Surface hardness can be described as the resistance of the material against vertical perforation (8). The hardness of the maxillofacial silicone elastomer is determined by the density of cross-links and the surface characteristics of polymer network (9). An ideal maxillofacial silicone elastomer should have an optimum hardness value to mimic the surrounding tissues (10).

Previous studies have evaluated the effect of artificial aging and real time aging on the mechanical and physical properties of different types of maxillofacial silicones. However, no previous study evaluated the effect of long-term dark storage on the hardness of nanoparticle added two types of room temperature vulcanized (RTV) maxillofacial silicone elastomers. Therefore, the purpose of this study was to evaluate the effect of long-term dark storage on the hardness of nanoparticle added two types of RTV maxillofacial silicone elastomers. The null hypotheses tested in this study were twofold; first, the natural aging would not affect the hardness of nanoparticle added maxillofacial silicone elastomers and second, Shore A hardness of the nanoparticle added specimens would be reduced after dark storage.

Materials and methods

Specimen preparation

The materials used in this study are given in Table 1. Platinum based A-2000 and A-2006 RTV type silicone elastomers were tested. A total of 64 silicone elastomer specimens (N=64) were fabricated from A-2000 and A-2006 silicones. Silane treated silica, fumed silica and titanium dioxide (TiO₂) nanoparticles were used as fillers. A metal mold was fabricated in accordance with the American Society for Testing and Materials (ASTM) D2240-68 standard for the standardization of the silicone specimens for the hardness tests.

For the fabrication of specimens in control group (Group 1), the homogenous silicone mixtures were prepared from A-2000 and A-2006 silicone elastomers, respectively. The ratio of the silicone elastomers were 1:1 for part A and part B of the silicones. A thixotropic agent, which prevents air bubble formation, was added to the silicone mixture and mixed by hand, according to the manufacturer's instructions. Thus, Group 1 with no addition of nanoparticles served as the control group for A-2000 and A-2006 silicone elastomers. For Group 2, 12 nm hydrophilic fumed silica nano particles were added at 10% concentration by volume to the silicone mixture. For Group 3, 12 nm silane-treated hydrophobic silica nanoparticles were incorporated to the silicone mixture at 10% concentration by volume. For Group 4, 30 nm TiO₂ nanoparticles were added to the silicone mixture at 10% concentration by volume. The final silicone mixture was poured to the metal mold and silicone specimens were polymerized. The manufacturer recommends the polymerization to take place at 75°C for 3 or 4 hours in stone molds and dry oven. They also

recommend higher polymerization degree and lesser time if the metal molds used. For standardization of the specimens, metal molds, instead of stone molds, and constant pressure with proper degree of temperature were selected. Therefore, the polymerization process was set for the specimens as 6 minutes in 60°C under a hydraulic press (HD80; Motor Operated, Hidroliksan, Konya, Türkiye) in metal molds, according to the method described in a previous study (1). Eight silicone specimens were fabricated for each study group (n=8). Thus, a total of 64 silicone specimens from A-2000 and A-2006 silicone elastomers (32 in each) were used in this study for the hardness tests.

Shore A hardness measurements

Silicone specimens in 30 mm diameter and 10 mm thickness were prepared in a metal mold in compliance with the ASTM D2240-68 standard (Figure 1). The hardness measurements of the specimens were made by using a digital Shore A durometer (Shore Leverloader, Duratronic, Akron, OH, USA). Three hardness measurements were taken from each specimen as Shore units and the average values were calculated as the final Shore A value, before and after the dark storage of the specimens.

Storage conditions

Dark storage performed for the silicon specimens included storing the specimens in room temperature 23°C±2°C and relative humidity in pigment free plastic bags. Specimens then placed in a lightproof wood box for 2-years. At the end of this period, specimens were removed and tested by using the digital Shore A durometer (Figure 2).

Statistical analysis

The collected data from all groups were imported to Statistical Package for the Social Sciences software version 20



Figure 1. Silicone specimens after polymerization process.



Figure 2. Shore A testing of the specimens.

(SPSS IBM Corp.; Armonk, NY, USA). The standard descriptive methods such as the mean, standard deviation, minimum and maximum were applied to determine the characteristics of the sample. All data were first evaluated with Levene's test for homogeneity of variances and with Kolmogorov-Smirnov for normality. Paired t-test was used to evaluate the differences between the initial and the final hardness values of each nanoparticle groups in each silicone material. Because the data was normally distributed, one-way analysis of variance (ANOVA) with Tukey's Honestly Significant Difference (HSD) tests pairwise comparisons was used to compare the nanoparticle groups in each silicone group, respectively. Confidence interval was set to 95% and p values less than 0.05 statistically significant.

Results

ANOVA results are presented as the mean and standard deviation in Table 2 and Table 3, and t-test results are presented in Figure 3 and Figure 4.

As can be seen from Table 2, ANOVA results revealed that statistically significant difference was found among groups after dark storage ($p < 0.001$). The lowest hardness value was observed in fumed silica group in A-2000 silicone elastomer. However, there was no significant difference between control and silica groups. While the highest hardness value was observed in TiO_2 , the significant difference was found between control and TiO_2 groups ($p = 0.003$). According to ANOVA results for the hardness values of A-2006 silicone (Table 3), there was statistically significant difference among the groups ($p < 0.001$). The lowest hardness value was observed in control group. Furthermore, while the highest hardness value was observed in silica group, there was not statistically significant difference between silica and silane groups in A-2006 silicone elastomer. According to paired t-test results, there was a significant difference between the hardness of each type of silicone and silicone subgroups before and the after storage ($p < 0.001$). Shore A hardness of all specimens significantly increased after dark storage.

Discussion

In this study, it was found that 2 years of dark storage adversely affected Shore A hardness of the silicone specimens. Furthermore, regarding after-storage specimens, nanoparticle incorporation did not reduce the hardness of the silicone elastomers as compared to control groups. The hardness values of silicone elastomers after 2-years dark storage varied from 47.28 to 22.75, for A-2000 and A-2006, respectively. Both silicone elastomers, with or without nanoparticles, demonstrated significant hardness increase after dark storage. However, Shore A values of stored specimens were found to be consistent with the hardness values of silicone elastomers reported by Veres *et al.* (1, 11).

Many studies evaluated Shore A hardness of silicone elastomers for periods of 2 (12), 6 (13-15) or 12 (16, 17) months with measurements taken at the initial and the final observation periods. Because the standard clinical longevity of the

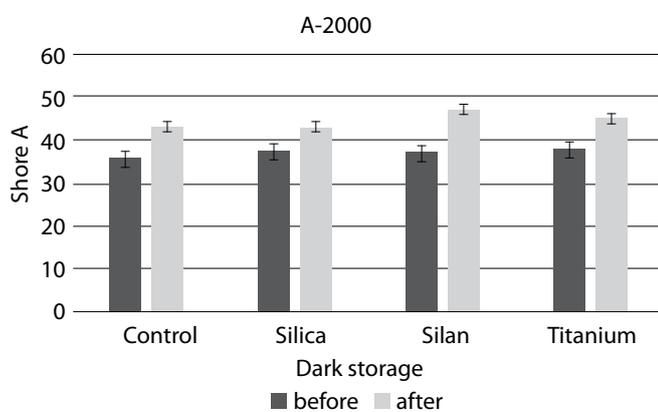


Figure 3. Paired t-test results, hardness (Shore A) values of A-2000 silicone before and after dark storage.

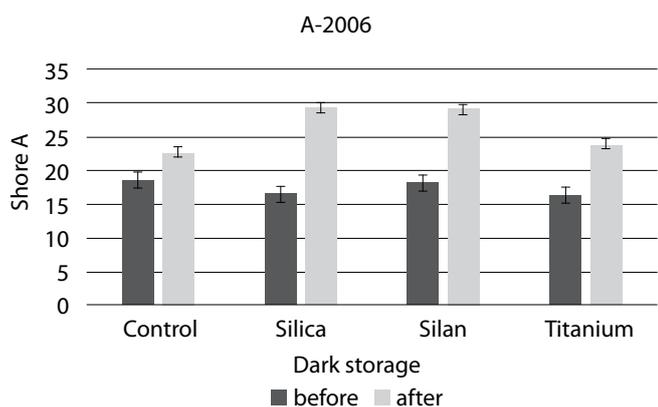


Figure 4. Paired t-test results, hardness (Shore A) values of A-2006 silicone before and after dark storage.

Table 1. Information on the materials used in this study

Material	Type	Manufacturer
RTV Silicone	A-2000	(Factor II Inc. Lakeside; AZ, USA)
RTV Silicone	A-2006	(Factor II Inc. Lakeside; AZ, USA)
Fumed Silica	Cab-O-Sil	(Factor II Inc. Lakeside; AZ, USA)
TiO ₂	30nanoTi	(Imicryl, Turkey)
Silanated silica	S-812	(Imicryl, Turkey)
Thixotropic agent	A-300-1 Thixo	(Factor II Inc. Lakeside; AZ, USA)

RTV: room temperature vulcanized

Table 2. Final Shore A values for A-2000 silicone elastomer

Groups	N	Mean	SD	Min	Max
Control	8	43.32 ^a	1.0	41.23	44.43
Silica	7	43.12 ^a	1.3	40.23	44.60
Silan	8	47.28 ^b	1.0	45.26	48.86
Titanium	8	45.39 ^c	.7	44.20	46.44
Total	31	44.70	1.9	40.23	48.86

Different superscript letters indicate the significant differences between groups
Means with same lowercase letters are not significantly different
SD: standard deviation

Table 3. Final Shore A values for A-2006 silicone elastomer

Groups	N	Mean	Std Dev	Min	Max
Control	8	22.75 ^a	.7	21.42	23.72
Silica	8	29.45 ^b	.6	28.53	30.16
Silan	8	29.26 ^b	.5	28.38	30.06
Titanium	7	23.91 ^c	1.0	22.50	25.22
Total	31	26.24	3.1	21.42	30.16

Different superscript letters indicate the significant differences between groups
Means with same lowercase letters are not significantly different
SD: standard deviation

facial prosthesis averages from 7 to 24 months (6, 18-22), it would be useful to evaluate the effect of time passage of at least 12-months on Shore A hardness of such silicone elastomers (22, 23). Therefore, the effect of long-term dark storage on the hardness value of silicone elastomers was evaluated in this study.

The relative hardness of a maxillofacial silicone elastomer should imitate the surrounding tissues and resemble the human skin (7). Facial prostheses during clinical service should be resistant and yet to soft and flexible to mimic the facial movements (24, 25). The acceptable limits of Shore A values for a facial silicone elastomer range from 25 to 55 units (26).

The reason of different values considered to be acceptable clinically is due to the hardness variations that exist in the maxillofacial area.

It was reported that physical changes of maxillofacial elastomers that occur during natural aging could result from polymerization by-products, initiators (15), pigments and other fillers (2, 27). In this study, nanoparticle fillers adversely affected the hardness values of silicones after dark storage. However, hydrophilic fumed silica nanoparticles decreased the hardness value of A-2000 silicone as compared to control group. Hydroxyl groups of the hydrophilic fumed silica could generate hydrogen bonds between the silica and silicone. Thus, fumed silica could increase the mechanical properties of silicones (28). Most studies reported that fumed silica nanoparticles could increase the mechanical properties of silicone elastomers (1, 29, 30).

Nano-oxide particles have been used as fillers in silicone elastomers to strengthen the mechanical properties of elastomers. By cross-linking reactions, nano-oxide particles could increase the surface energy of silicone matrix, which leads to a reinforced matrix structure (31, 32). In recent studies, titanium dioxide nanoparticles were found to increase the mechanical properties of silicone elastomers (1, 7, 33). According to the results of this study, it could be stated that fumed silica nanoparticles might be effective on the mechanical properties of A-2000 silicone elastomer while TiO₂ nanoparticles might be effective on the mechanical properties of A-2006 silicone elastomer.

Most studies on silicone elastomers subjected to dark storage are generally based on color stability (2, 23, 25, 34, 35). However, limited research investigated the mechanical properties of silicone elastomers subjected to dark storage (17, 25, 27, 36). Furthermore, our study has a main difference with recent studies in which we investigated the effect of nanoparticle addition on the hardness of silicone elastomers after being subjected to dark storage.

Hardness increment during dark storage could result from continuous vulcanization (12, 36, 37) of the silicone elastomers due to the presence of nanoparticles. A possible explanation of hardness increment could be a mechanism that may start due to oxygen intake during dark storage and generates cross-linkers which cluster in the silicone matrix, leading to denser network and higher hardness for silicone materials (17, 38).

The hardness of the silicone elastomers is controlled by the surface characteristics of the polymer network and the density of crosslink as reported by Polyzois *et al.* (17) Furthermore, the density of the cross-linkers could affect the length of the polymer chain (39) which results in degradation of mechanical properties of silicon elastomers in time. Therefore, another possible reason for increased hardness of nanoparticle added silicones could be that nanoparticles maximize the network of silicone matrix, lengthen of the polymer chain, leading to increased hardness values.

Lai and Hodges (40) and Raptis *et al.* (41) reported that the silicone elastomers are not completely vulcanized in stone molds. Furthermore, stone molds have more surface irregularities than the metal molds do (1). Accordingly, new generation silicone elastomers are polymerized in metal molds (40).

Although stone molds can imitate the clinical fabrication techniques, metal molds were preferred for the polymerization process of the silicone elastomers to provide accurate and standard data in this study.

Various studies have used nano particles as fillers at different concentrations. Fillers used in this study were at 10 % by volume, which is consistent with previous studies (30, 33) and it is based on the results of a recently published article (1), in which the mechanical properties of silicones were evaluated after nanoparticle incorporation. Thus, different concentrations of nano particles could lead to differences in mechanical and physical properties of silicone elastomers. Therefore, future research should address the effects of adding such nanoparticles at different concentrations on the mechanical and physical properties of maxillofacial silicone elastomers subjected to aging process.

Conclusion

Within the limitations of this *in vitro* study, it can be stated that the hardness of A-2000 and A-2006 silicone elastomers increased after 2-years dark storage. On the other hand, both silicone elastomers, with or without nanoparticles, showed clinically acceptable Shore A hardness values even after dark storage. Nanoparticle addition did not prevent silicone elastomers from hardening effects of time and, finally, A-2000 silicone revealed maximum hardness values in all study groups.

Ethics Committee Approval: Ethics committee approval was received for this study from the ethics committee of 12.01.2012 with the number 2012/01.

Informed Consent: There is no need for an informed consent form for the current *in vitro* study.

Peer-review: Externally peer-reviewed.

Author Contributions: PÇ designed the study, generated, gathered and analyzed the data, wrote and approved the final version of the paper.

Conflict of Interest: The author have no conflicts of interest to declare.

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Türkçe öz: Maksillofasiyal silikonlarda Shore A sertlik ölçümü: karanlık ortam ve nanopartiküllerin etkisi. Amaç: Nanopartikül ilavesinin maksillofasiyal silikonların sertliğine olan etkisi hakkında yeterince çalışma bulunmamaktadır. Bu çalışmanın amacı, farklı nanopartikül ilavesi ve iki yıl karanlık ortam yaşlandırmasının maksillofasiyal silikon elastomerlerin sertliğine olan etkisini incelemektir. Gereç ve Yöntem: Çalışmada RTV tip A-2000 ve A-2006 silikon elastomerler test edilmiştir. Silanlanmış silika, tütsülenmiş silika ve titanyum dioksit nanopartikülleri hacimce %10 oranında doldurucu olarak kullanılmıştır. Her bir silikondan 30 x 10 mm boyutlarında sekiz örnek olmak üzere, kontrol grubu dahil toplam 64 silikon örnek hazırlanmıştır. İlk Shore A sertlik değerleri alınan örnekler oda sıcaklığında karanlık ortamda iki yıl boyunca saklanmış ve örneklerin yaşlandırma sonrasına ait ikinci Shore A değerleri kaydedilmiştir. Veriler istatistiksel olarak analiz edilmiştir. Bulgular: Her tip silikon için, gruplar arasında sertlik değerleri açısından istatistik-

sel olarak anlamlı farklar gözlenmiştir ($p < .001$). Yaşlandırma sonrası; A-2000'e ait tütsülenmiş silika en düşük sertlik değerleri verirken, kontrol grubu ile arasında anlamlı bir fark bulunamamıştır. A-2006 için, kontrol grubu en düşük sertlik değeri verirken, en yüksek sertlik değeri tütsülenmiş silika grubunda gözlenmiştir. A-2006 'ya ait tütsülenmiş silika ve silanlanmış silika grupları arasında istatistiksel olarak anlamlı bir fark gözlenmemiştir. Sonuç: Yaşlandırma işlemi sonrasında maksillofasiyal silikonlara ait sertlik değerleri klinik olarak kabul edilebilir değerler arasında kalmıştır. Bununla birlikte, nanopartikül ilavesi silikon elastomerleri yaşlandırma işlemi sırasında ortaya çıkan sertlik artışına karşı koruyamamaktadır. Anahtar kelimeler: Yaşlandırma; sertlik; nanopartiküller; silikon elastomerler; Shore A

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